A novel temperature control method for shortening thermal cycling time to achieve rapid polymerase chain reaction (PCR) in a disposable polymer microfluidic device.

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A NOVEL TEMPERATURE CONTROL METHOD FOR SHORTENING THERMAL CYCLING TIME TO ACHIEVE RAPID POLYMERASE CHAIN REACTION (PCR) IN A DISPOSABLE POLYMER MICROFLUIDIC DEVICE

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Abstract — We present a new temperature control method capable of effectively shortening the thermal cycling time of polymerase chain reaction (PCR) in a disposable polymer microfluidic device with external heater and temperature sensor. The method employs optimized temperature overshooting and undershooting steps to achieve a rapid ramping between the temperature steps for DNA denaturation, annealing and extension. The temperature dynamics within the microfluidic PCR chamber was characterized and the overshooting and undershooting parameters were optimized using the temperature dependent fluorescence signal from Rhodamine B. The method was validated with PCR amplification of mecA gene (162 bp) from Methicillin-resistant Staphylococcus aureus bacterium (MRSA), where the time for 30 cycles was reduced from 50 min (without over- and undershooting) to 20 min.

Keywords: Temperature control method, Polymerase chain reaction (PCR), Polymer microfluidic device

I - Introduction

With the potential of low cost, rapid reaction and multi-functional integration, microfluidic devices using PCR for nucleic acid analysis have been extensively exploited for a wide range of applications [1-2], such as pathogen sensing [3] and point-of-care diagnostics [4-5].

Using silicon microfabrication technology, ultra fast real-time PCR has been achieved with 40 cycles in less than 6 minutes [6]. However, the high cost of the microfabrication process hindered commercialization of this type of microfluidic device. Low-cost fabrication technologies, such as injection moulding, have been used recently to fabricate disposable polymer microfluidic devices for DNA analysis [7].

In comparison to the silicon, polymer materials have 1000 times lower thermal conductivity, which substantially slows down the heat transfer, especially when external heaters are used to heat the reaction chamber. This considerably prolongs the time for PCR cycling. However, by optimizing the heating and cooling control, a rapid PCR is still achievable, even in polymer microfluidic devices with external heaters.

In this work, we present a new method featuring temperature overshooting for heating and undershooting for cooling to obtain a rapid ramping between the three temperature steps for PCR. The work is part of a microfluidic control platform with a re-usable micro-pump/valve actuator [8] and a re-usable external silicon heater for DNA sample preparation and PCR amplification in a disposable microfluidic TOPAS® cyclic olefin copolymer chip for rapid pathogen detection.

II– Experimental

A. Design of PCR Thermal Cycling Platform

Figure 1a illustrates the design of PCR thermal cycling platform. An external silicon heater (10 mm × 13 mm × 0.35 mm) with integrated Pt thin film resistive heater and temperature sensor on the bottom side is used to control the temperature in the PCR reaction chamber of an injection moulded TOPAS® chip (Figure 1b). The silicon heater is mounted on a printed circuit board (PCB) with conductive silver epoxy glue, and the PCB is mounted in a recess machined in an aluminum plate.

Figure 1: An illustration (a) and a top view (b) of the thermal cycling platform.

The disposable TOPAS® chip is clamped under a polycarbonate clamping plate. The clamping plate has a hole above the PCR chamber through which compressed air (3.5 bar, 22 °C) can be passed to cool the top of the TOPAS® chip during PCR. Compressed air is
also used to cool the silicon heater from bottom of the platform. Figure 1b shows a top view of the thermal cycling platform and a silicon heater (top and bottom view). The PCR chamber in the injection moulded TOPAS® chip (1 mm thick) is sealed with a TOPAS® film (250 µm thick) using ultrasonic welding. The reaction chamber has a dimension (depth×width×length) of approximately 0.4×3.4×5 mm³ (~6 µL).

B. Steady-State On-Chip Temperature Measurement

Since the temperature sensor is integrated on the external heater, but not in the chip, non-contact methods were used to characterize the temperature in the PCR chamber. An infrared (IR) camera was used to monitor the steady-state temperature on the top surface of the TOPAS® chip ($T_{\text{top}}$), when heater temperatures ($T_{\text{heat}}$) was changed from 50 to 100 °C with a step of 10 °C. At each step, to ensure the system reaches thermal equilibrium, the heater was kept at each set temperature for 15 minutes before $T_{\text{top}}$ was measured.

In order to characterize the temperature in the PCR chamber ($T_{\text{cham}}$), measurement on the melting points of PCR amplicons of different lengths has been carried out both on-chip and in a conventional real-time PCR machine (Chromo4, Bio-Rad, Denmark) as a reference ($T_m$). PCR amplicons were amplified in the conventional PCR machine first and then filled into the TOPAS® chips. When the DNA fragments melt in the TOPAS® chip, $T_m$ is equal to $T_{\text{cham}}$, and the heater temperature at this moment was marked as $T_{\text{m,heater}}$. During the measurement, $T_{\text{heat}}$ was changed in steps of 0.2 °C with a dwell time of 32 s at each step. No difference was found between sweeping up and down in temperature, indicating that the dwell time was sufficiently long to reach thermal equilibrium. The amplicons used were: (1) PVL gene of MRSA (83 bp, $T_m=78$ °C); (2) mecA gene of MRSA (162 bp, $T_m=78.8$ °C); (3) Hiporicase gene of Campylobacter jejuni (150 bp, $T_m=79.3$ °C); (4) spa gene of MRSA (400 bp, $T_m=84.4$ °C); (5) 16S RNA gene of Campylobacter (300 bp, $T_m=86.4$ °C).

C. Dynamic On-Chip Temperature Measurements

The temperature dynamics within the PCR chamber was monitored in real-time using the temperature dependent fluorescence signal from a 25 µM Rhodamine B (Rhb) solution in the chamber. The fluorescence of Rhb decreases as a function of increasing temperature. The intensity was converted to temperature using a three point calibration based on a comparison between steady-state fluorescence signals and steady-state temperatures in the chamber obtained from a 1-dimensional thermal model of the system.

D. Temperature Over- and Undershooting Method and its Validation

The characterization of the dynamic response of the temperature in the chamber was employed to optimize the setting of $T_{\text{heat}}$ in this new temperature control method for PCR. This method features a step with temperature overshooting of several degrees above the target set point for the extension and denaturing steps, as well as a step with temperature undershooting below the target temperature set point for the denaturing step.

The optimized temperature over- and undershooting method was validated with the on-chip PCR amplification of the mecA gene of MRSA.

III – Results and Discussion

A. Steady-State On-Chip Temperature Measurement

Figure 2 shows the IR camera measured steady-state temperature $T_{\text{top}}$ as a function of the heater temperature $T_{\text{heat}}$. It also shows the reference melting temperatures $T_m$ as function of the $T_{\text{m,heater}}$ for the five studied PCR amplicons.

From Figure 2 it is seen that $T_{\text{top}}$ systematically lies below $T_{\text{heat}}$ with a difference that increases linearly with increasing $T_{\text{heat}}$ (e.g. 5 °C when $T_{\text{heat}} = 100$ °C). This is in agreement with the expectations from a 1D thermal circuit model of the system and also shows that the largest temperature gradient occurs between the top surface of the chip and the surroundings. The values of $T_m$ ($T_{\text{cham}}$) vs. $T_{\text{m,heater}}$ as expected, lie systematically between $T_{\text{top}}$ and $T_{\text{heat}}$ and are approximately linearly related to $T_{\text{heat}}$. These values provide an independent calibration of the temperature in the PCR chamber and it is found (in agreement with expectations from modeling) that near the investigated melting temperatures, $T_{\text{cham}}$ is about 1.6 °C lower than the heater temperature $T_{\text{heat}}$ when $T_{\text{heat}} \approx 85$ °C.

We further tested the reproducibility of on-chip measurements of melting points when the measurements were carried out in different chips. The variability in measurements from chip to chip may originate from chip fabrication variations and the quality of the thermal contact to the chip. Figure 3 shows the on-chip melting curves obtained from six different chips containing PCR amplicons of the PVL gene of MRSA (83 bp, $T_m=78$ °C). The chips were prepared with identical procedures and the experiments were carried out under identical conditions.
The measured Rhodamine B fluorescence for the three temperature steps required to measure the melting point. This indicates that a reproducible thermal contact and an efficient heat transfer to the disposable TOPAS™ chip through the bottom of the chip have been obtained in this system.

B. Dynamic On-Chip Temperature Measurement and Optimization of Under- and Overshooting Method

Dynamic on-chip measurements of \( T_{cham} \) and the optimization of temperature under- and overshooting for the PCR amplification of Campylobacter DNA (150 bp and 300 bp) were carried out. The optimal values of \( T_{heat} \) for these steps were found using a commercial PCR machine and the corrections based on Figure 2 to 54.5 ºC, 73 ºC and 96.5 ºC, respectively. Figure 3 shows the dynamic on-chip temperature measurements results obtained using Rhodamine B fluorescence for the three temperature steps required to carry out the PCR cycling. The measured Rhodamine B fluorescence signal \( (F_N) \) was normalized to the value when the chamber reaches thermal equilibrium. When no over- or undershooting is used, the PCR chamber is not able to reach thermal equilibrium in 25-30 s of dwell time. This is due to the low thermal conductivity of the polymer and the significant thermal mass of the chip. To decrease the time required to reach thermal equilibrium in the PCR chamber, we systematically investigated controlled temperature over- and undershooting, where a higher or lower value of \( T_{heat} \) is used for a fixed period of time of 3 s. Figure 4 shows the results of these investigations for different values of the over- and undershooting temperatures. The optimal parameters of

![Figure 3: Melting curve analysis of PCR amplicon of PVL gene from MRSA in 6 different TOPAS chips. Top: Fluorescence intensity \( (I) \) drops substantially at melting point. Bottom: Negative first derivative of the fluorescence intensity \( (-d(I)/dT) \) shows the on-chip measured melting point \( (Tm,heater) \).](image)

![Figure 4: Rhodamine B fluorescence signal \( (F_N) \) for optimization of (a) overshooting from 54.5 ºC (annealing step) to 73 ºC (extension step), (b) from 73 ºC to 96.5 ºC (denaturing step), and (c) undershooting from 96.5 ºC to 54.5 ºC.](image)
Table 1: Heater temperature and dwell time setting for PCR amplification of mecA Gene of MRSA.

<table>
<thead>
<tr>
<th>Step</th>
<th>$T_{\text{heat}}$ [°C]</th>
<th>PCR 01/02 [s]</th>
<th>PCR 03 [s]</th>
<th>PCR 04 [s]</th>
<th>PCR 05 [s]</th>
</tr>
</thead>
<tbody>
<tr>
<td>Initial activation</td>
<td>110</td>
<td>6</td>
<td>6</td>
<td>6</td>
<td>6</td>
</tr>
<tr>
<td>step</td>
<td>95.5</td>
<td>182</td>
<td>182</td>
<td>182</td>
<td>182</td>
</tr>
<tr>
<td>Annealing</td>
<td>52</td>
<td>5 (1.9)</td>
<td>5 (1.9)</td>
<td>5 (1.9)</td>
<td>3 (1.9)</td>
</tr>
<tr>
<td>Extension</td>
<td>60</td>
<td>22 (0.8)</td>
<td>12 (0.8)</td>
<td>7 (0.8)</td>
<td>4 (0.8)</td>
</tr>
<tr>
<td>Denaturation</td>
<td>81</td>
<td>5 (0.2)</td>
<td>5 (0.2)</td>
<td>5 (0.2)</td>
<td>3 (0.2)</td>
</tr>
<tr>
<td>Cycle time [s]</td>
<td>108</td>
<td>22 (0.6)</td>
<td>12 (0.6)</td>
<td>7 (0.6)</td>
<td>4 (0.6)</td>
</tr>
</tbody>
</table>

Figure 5 shows the dynamic temperature response of the heater and PCR chamber for the PCR 04 conditions in Table 1. For the heater, the heating and cooling rates are approximately 14 °C/s and 9 °C/s, respectively, and for the PCR chamber heating and cooling rates of about 4.3 °C/s and 5 °C/s are achieved.

Figure 6 shows measured real-time PCR fluorescence intensity vs. cycle number for the conditions in Table 1. The figure indicates that the mecA gene is amplified efficiently with a relatively high yield for conditions PCR 01 to PCR 04, where PCR 04 has the shortest total run time of about 20 min for 30 cycles.

The identity of the PCR product was verified by gel electrophoresis (Figure 7). Without temperature over- and undershooting a total run time of 50 min for 30 PCR cycles is required for efficient amplification.

Figure 7: Gel electrophoresis analysis of 5 PCR amplicons reveals the successful amplification of specific mecA gene of MRSA. From left to right, lane L: ladder, lane 1-5: PCR 01-05, lane 6: empty, lane 7-11: repeat of PCR 01-05, lane 12: empty. The size of the product is 162 bp.

IV - Conclusion
An overshooting and undershooting control method has been investigated and carefully optimized to obtain a rapid temperature ramping during PCR on a disposable polymer chip using external heaters. The experimental results proved that this method is able to effectively shorten the PCR thermal cycling time in the investigated polymer chip by ~50%, compared to PCR setting without over/undershooting in the same chip.

V – Acknowledgements
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