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Rocking Convex Array used for 3D Synthetic Aperture Focusing

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Abstract—**Volumetric imaging can be performed using 1D arrays in combination with mechanical motion. Outside the elevation focus of the array, the resolution and contrast quickly degrade compared to the azimuth plane, because of the fixed transducer focus. The purpose of this paper is to use synthetic aperture focusing (SAF) for enhancing the elevation focusing for a convex rocking array, to obtain a more isotropic point spread function.**

This paper presents further development of the SAF method, which can be used with curved array combined with a rocking motion. The method uses a virtual source (VS) for defocused multi-element transmit, and another VS in the elevation focus point. This allows a direct time-of-flight (ToF) to be calculated for a given 3D point. The method is evaluated using simulations from Field II and by measurements using the RASMUS experimental scanner with a 4.5 MHz convex array (GE Kretztechnik, Zipf, Austria). The array has an elevation focus at 60 mm of depth, and the angular rocking velocity is up to 140°/s. The scan sequence uses an f_{prf} of 4500 - 7000 Hz allowing up to 15 cm of penetration. The full width at half max (FWHM) and main-lobe to side-lobe ratio (MLSL) is used as quantitative measurements.

The elevation FWHM for simulated scatterers placed at depths of 30 to 140 mm of depth were improved by 26.4% on average, and the MLSL ratio was improved by an average of 8.49 dB for the scatterers using 3D SA focusing. The elevation FWHM for a measured wire phantom was improved by 33.8% on average by applying 3D SA focusing. *In-Vivo* measurements show an improvement in C-scans matching what is found in simulations and wire phantoms.

The method has shown the ability to improve the elevation focus and contrast for a convex rocking array. This was shown for simulations and for phantom and *In-Vivo* measurements using commercially available equipment.

I. Introduction

Rocking convex linear arrays are used to acquire 3D volume ultrasound (US) images. These arrays are available from commercial manufacturers, and many commercial scanners are able to use them them to gather a 3D dataset. These arrays are commonly used for abdominal scans to visualize organs and fetuses. The 3D volumes are created by imaging slices and stacking these to a volume. The volume has a good lateral-depth resolution, but poor elevation resolution because of the small elevation aperture and the fixed lens focus.

Using synthetic aperture (SA) focusing technique to improve the resolution of a fixed focus transducer has been shown feasible in [1]. This has further been used in [2]–[4] with linear and phased array transducers, to allow for both lateral and elevation focusing. Here a set of planes are beamformed with SA focusing, generating a set of lateral scan-lines. The volume is created by beamforming the scan-lines in elevation by assuming that the elevation focus is a virtual source. Previous work has shown a significant increase in both elevation resolution, contrast, and signal to noise ratio (SNR) when applying this 2-step elevation beamforming method.

This paper presents the implementation of a 3D time of flight (ToF) calculation on a rocking convex array. The ToF method has previously been used for improving the elevation resolution for a translated linear array [5]. The mothod allows for a precise ToF calculation for lateral and elevation beamforming, using only a single beamforming step. This removes the requirement for beamforming in-plane points at the Nyquist criteria, and only uses points required for the volume. Section II will describe the equations and theory used in the method, the measurement setup is described in Section III, and Section IV will show the results from both simulation and measurements. The paper is concluded in Section V.

II. Theory

SA focusing used from linear arrays is traditionally done by calculating the ToF for a spherical wave emitted by a single element, allowing each emission to contribute to the focusing of the entire insonified region. As a single element emissions gives a low SNR, virtual sources (VS) [3], [6], [7] and frequency modulation [8] are used to increase the emitted energy.

The method presented in [5] describes the ToF calculation for a given 3D-point for a linear array. This method has been implemented for a convex rocking array. To allow for a calculation using the rocking array, the ToF will be calculated using a rotated coordinate system. $[x, y, z]$ will denote the lateral, elevation, and depth direction, respectively. Two rotations are performed to place the emitting virtual source at the origo in the $x - y$ direction with the propagation direction along the

z axis. The first rotation is to counter the rocking motion, changing coordinates by

$$\hat{r}_p = (\vec{r}_p - \vec{v}_{\text{ele,origo}}) \cdot \mathbf{M}(\phi) + \vec{v}_{\text{ele,origo}}, \qquad (1)$$

where $\vec{r}_p$ is the point of interest, $\hat{r}_p$ is the rotated point, $\vec{v}_{\text{ele,origo}}$ is the point of rotation for the elevation rocking motion, and $\mathbf{M}(\phi)$ is the rotation matrix around the x-axis, which is dependent on the tilt of the array in the elevation direction. The second rotation is done by

$$\tilde{r}_p = (\hat{r}_p - \vec{v}_{\text{lat,origo}}) \cdot \mathbf{M}(\theta) + \vec{v}_{\text{lat,origo}}, \qquad (2)$$

where $\hat{r}_p$ is the point of interest rotated in the $y-z$ plane, $\tilde{r}_p$ is the final rotated point, $\vec{v}_{\text{lat,origo}}$ is the point of origin for the convex array curvature, and $\mathbf{M}(\theta)$ is the rotation matrix along the rotated y-axis, where θ is equal to the angle between the center of the array and the virtual transmit source.

The process of calculating the ToF is a two-fold process, as a VS is used both in the lateral and the elevation direction. The process is shown in Fig. 1, using the rotated coordinate system, where the point $\tilde{r}_p$ is the desired beamformed point, the dotted lines in the $x-z$ plane show the acceptance angle for the transmit VS and the dashed lines show the acceptance angle for the VS placed at the elevation focus. The point $\tilde{r}_p$ is projected onto the $x-z$-plane by letting the depth of the point be the distance traveled by the sound on a plane orthogonal to the $x-z$-plane, by placing a VS at the elevation focus on the same lateral position as $\tilde{r}_p$. The depth of the new point will be given by

$$z_{\text{proj}} = \sqrt{\tilde{r}_{p,y}^2 + (\tilde{r}_{p,z} - \tilde{z}_{ele})^2} \cdot sign(\tilde{r}_{p,z} - z_{ele}) + z_{ele}, \qquad (3)$$

where $\tilde{r}_{p,y}, \tilde{r}_{p,z}$ is the elevation and depth position of $\tilde{r}_p$ relative to the transducer and z_{ele} is the depth of the elevation focus. This virtual point is used for the ToF calculation using in-plane SA focusing. The virtual point, denoted $\vec{r}_v$, will have the coordinates $(r_{p,x}, 0, z_{ele})$. The equation for the total ToF for a transmission to the m'th receive element is given by

$$t_{\text{ToF},m} = \frac{|\tilde{r}_v - \tilde{r}_{VS}| + |\tilde{r}_v - \tilde{r}_{rcv,m}|}{c}, \qquad (4)$$

where $\tilde{r}_{VS}$ is the position of the transmit VS, $\tilde{r}_{rcv,m}$ is the position of the m'th receiving element, and c is the speed of sound. The path is shown by the solid black line in Fig. 1. The signal amplitude for a single point is given by summing the received signals at the time instances calculated by (4), which yields

$$s(\vec{r}_p) = \sum_{m=1}^{M} \sum_{n=1}^{N} a_{m,n} \cdot g_{m,n}(t_{ToF,m}), \qquad (5)$$

where $a_{m,n}$ is the apodization and $g_{m,n}$ is the signal for the m'th receive channel of the n'th emission. M is the number of receive elements and N is the number of transmit VS's..
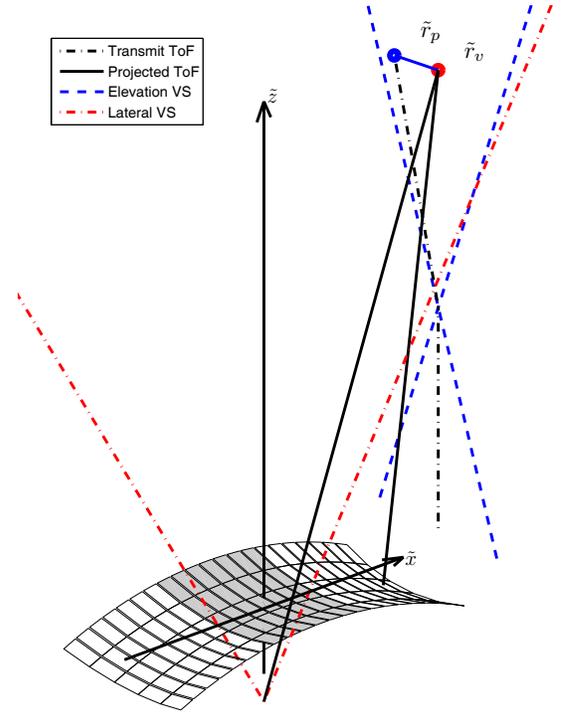

Figure 1. Illustration of the ToF calculation. Red dotted lines are transmit VS acceptance angle, blue dashed lines are elevation focus acceptance angle, the dotted black line is transmit ToF for the beamformed point, and solid black line is the total ToF for the projectet point. The blue point $\vec{r}_p$ is the desired beamformed point, and the red point $\vec{r}_v$ is the virtual projected point.

III. MEASUREMENT SETUP

All measurements were done with the RASMUS experimental scanner available at the Center for Fast Ultrasound imaging (CFU). RASMUS is an abbreviation for Remotely Accessible Software configurable Multi-channel Ultrasound Sampling system, and was designed as a very flexible US system capable of transmitting arbitrary waveforms and storage of raw array channel data. A more detailed description is found in [9]. The transducer used is a convex array with a stepping motor to allow for a continuous back and forth rocking motion. The rocking system is controlled from a separate control box. A synchronization is attained by measuring a trigger signal emitted from the control box on the RASMUS system. Different measurements parameters are used, and will be referred to by a number in Table II. The transducer parameters are the same for all measurements and simulations and given in Table I. The parameters and the movement profile for the simulations are taken from a similar measurements on the RASMUS system.

IV. RESULTS

To evaluate the methods ability to improve elevation resolution, the full width at half max (FWHM) and main-lobe to side-lobe ratio (MLSL) is calculated for a set of simulated scatterers and for measurements performed on a wire phantom. The main-lobe width used to calculate the MLSL is defined at

Table I
TRANSDUCER PARAMETERS.

Number of transducer elements	128
Center frequency, f_0	4.4 MHz
Transducer element pitch angle	0.268
Transducer element height	11 mm
Elevation focus	62 mm
Convex curvature radius	38.9 mm
Rocking radius	22.6 mm

Table II
MEASUREMENT PARAMETERS.

Scan number	1	2	3
Elements in virtual source	7	7	7
Emissions for full STA	80	80	80
Lateral VS Focusing F$^{\#}$	$-\frac{1}{2}$	$-\frac{1}{2}$	$-\frac{1}{2}$
FM-Chirp length	15 μs	15 μs	15 μs
Scan depth	160 mm	100 mm	145
Receive apodization	Hamming	Hamming	Hamming
Receive F$^{\#}$	2	2	2
Rocking sector	35°	35°	35°
f_{prf}	4500	7000	5000
Volumes per second	3.5	3.8	3.5

-20 dB for the PSF created with 3D SA focusing. In addition, a C-scan of an *In-Vivo* measurement is shown with and without 3D SA focusing.

The simulation is performed using the scan number 1 parameters in Table II. Fig. 2 shows the FWHM for a set of simulated scatterers between 30 mm and 140 mm of depth, which shows the methods ability to synthesize a larger aperture in the elevation direction. The improvement in FWHM is on average 26.4%. The method is not able to synthesize a constant F$^{\#}$ regardsless of depth, which is assumed to be caused by the high physical F$^{\#}$ of the transducer as well as the rocking motion. Fig. 3 shows the MLSL for the same simulated scatterers. The gain in MLSL is 8.49 dB on average. Fig. 4 shows the projected PSF at a depth of 80 mm. The
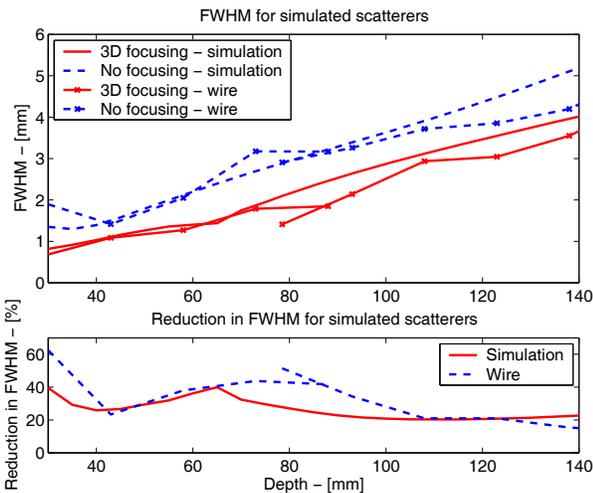

Figure 2. FWHM for simulated scatterers and measured wires with and without 3D SA focusing. The gain is calculated for both the measured and simulated scatterers.
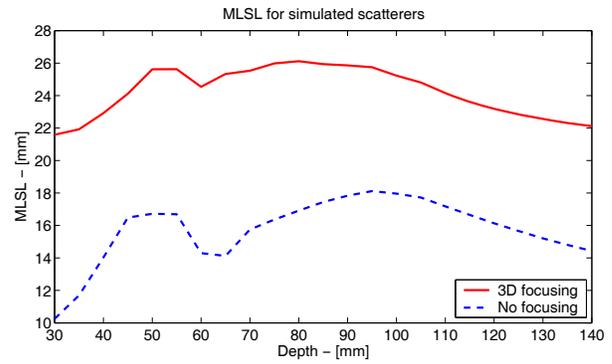

Figure 3. MLSL for simulated scatterers with and without 3D SA focusing.
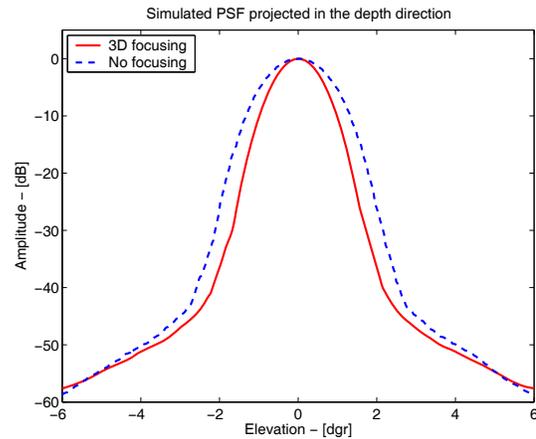

Figure 4. Simulated PSF at 80 mm of depth with and without 3D SA focusing.

mehod can be seen to improve the width of the PSF for all levels down to appr. -50 dB, in which the PSF without 3D SA focusing has slightly lower side-lobes.

A wire phantom was measured twice at different depths. The measurements are performed using the parameters from scan number 1 and 2, found in Table II. The two measurements are combined even though there is a change in the f_{prf}. Fig. 2 shows the FWHM for two measurements of a wire phantom on top of the results from the simulated scatterers. The evolution of the FWHM is very similar to the simulated scatterers, and the FWHM is almost the same value. The average improvement in FWHM for the measured scatterers is 33.8%, and is overall very similar to the simulated result.

Fig. 5 show the measured PSF in the elevation direction. The PSF is slightly smaller in width, but is otherwise comparable to the simulated PSF. The results shows a good correlation between the simulated and measured response, which validates the methods use for equipment readily available from commercial systems.

The C-scan of an *In-Vivo* measurement is shown in Fig. 6 and 7. The scan is showing the liver of a healthy 26 year old male volunteer. To the right in the middle is a vein, but of most interest is the speckle in the liver. This clearly shows a reduction in the elevation direction, confirming the simulation
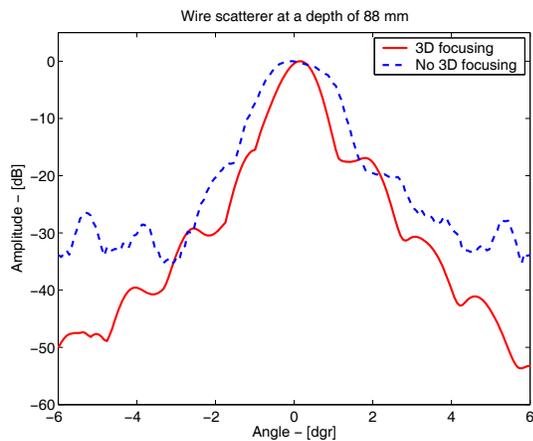
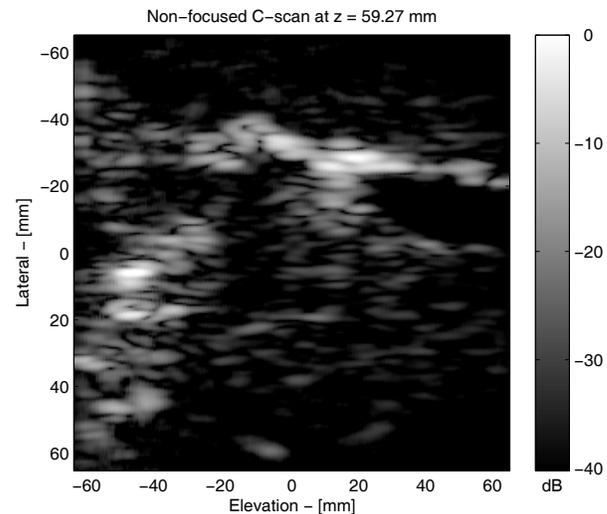Figure 5. Measured PSF at 88 mm of depth with and without 3D SA focusing.

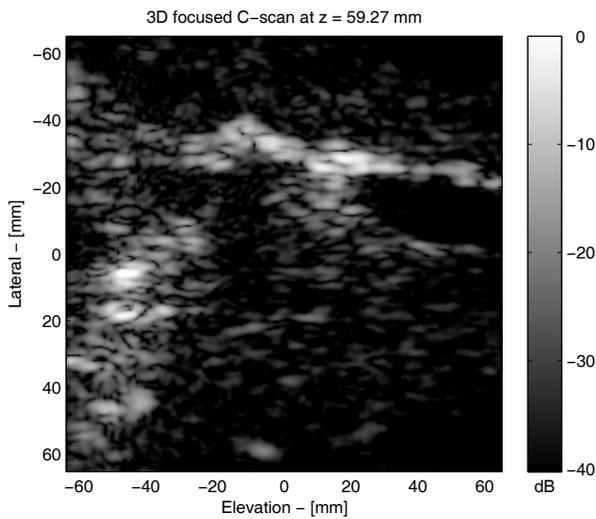Figure 6. *In-Vivo* measurement of liver in a healthy 26 year old male volunteer.

Figure 7. *In-Vivo* measurement of liver in a healthy 26 year old male volunteer.

and wire phantom measurements.

V. CONCLUSION

The method for 3D synthetic aperture focusing has been successfully implemented for a rocking convex array. The method is not able to maintain a constant $F^{\#}$, but shows an average improvement to the FWHM of 26.4% for simulated scatterers and 33.8% for a measured wire phantom. The simulated scatterers show a reduction in the width of the PSF between 0 dB and -50 dB, after which the amplitude is comparable. A C-scan of an *In-Vivo* measurement also shows the expected inprovement in the elevation direction.

The results presented in this paper proves the viability of the method to improve the contrast and resolution of real-time 3D ultrasound data acquisition using commercially available equipment.

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